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Construction of lymph nodes-targeting tumor vaccines by using the principle of DNA base complementary pairing to enhance antitumor cellular immune response



Yongchao Zha^{1†}, Li Fu^{1†}, Zonghua Liu^{1*}, Jiansheng Lin^{2*} and Linghong Huang^{1*}

Abstract

Tumor vaccines, a crucial immunotherapy, have gained growing interest because of their unique capability to initiate precise anti-tumor immune responses and establish enduring immune memory. Injected tumor vaccines passively diffuse to the adjacent draining lymph nodes, where the residing antigen-presenting cells capture and present tumor antigens to T cells. This process represents the initial phase of the immune response to the tumor vaccines and constitutes a pivotal determinant of their effectiveness. Nevertheless, the granularity paradox, arising from the different requirements between the passive targeting delivery of tumor vaccines to lymph nodes and the uptake by antigen-presenting cells, diminishes the efficacy of lymph node-targeting tumor vaccines. This study addressed this challenge by employing a vaccine formulation with a tunable, controlled particle size. Manganese dioxide (MnO₃) nanoparticles were synthesized, loaded with ovalbumin (OVA), and modified with A₅₀ or T₂₀ DNA single strands to obtain $MnO_2/OVA/A_{50}$ and $MnO_2/OVA/T_{20}$, respectively. Administering the vaccines sequentially, upon reaching the lymph nodes, the two vaccines converge and simultaneously aggregate into MnO₂/OVA/A₅₀-T₂₀ particles through base pairing. This process enhances both vaccine uptake and antigen delivery. In vitro and in vivo studies demonstrated that, the combined vaccine, comprising MnO₂/OVA/A₅₀ and MnO₂/OVA/T₂₀, exhibited robust immunization effects and remarkable anti-tumor efficacy in the melanoma animal models. The strategy of controlling tumor vaccine size and consequently improving tumor antigen presentation efficiency and vaccine efficacy via the DNA base-pairing principle, provides novel concepts for the development of efficient tumor vaccines.

Keywords Tumor immunotherapy, Tumor vaccines, Lymph node targeting, Cellular immunity

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Introduction

In recent years, tumor immunotherapy has revolutionized the conventional paradigm of tumor treatment [1, 2]. Notably, tumor vaccines have gained growing interest owing to their outstanding ability to initiate tumor-specific immune responses and establish enduring immune memory [3, 4]. Nonetheless, current tumor vaccines usually cannot trigger efficient cellular immune responses and do not meet the demands of effective tumor therapy [5]. Low antigen presentation efficiency in the process of the intricate immune response to tumor vaccines is deemed a critical bottleneck that constrains the magnitude of the vaccine's efficacy [6, 7]. The scarcity of antigen-presenting cells (APCs) in the peripheral tissues at conventional vaccination sites seriously hampers the capture and presentation of tumor antigens. Consequently,

the administered tumor vaccines primarily passively diffuse to the adjacent draining lymph nodes, where they can be captured by the resident APCs, realizing antigen presentation [8, 9]. Lymph nodes house diverse immune cells, including APCs, B lymphocytes, T lymphocytes, and natural killer cells. They serve as vital organs for immune surveillance, regulation, and activation [10]. Notably, lymph nodes harbor a substantial population of phagocytic dendritic cells (DCs) known for their proficiency in cross-presentation [11]. This refers to presenting exogenous antigens to CD8⁺ T cells via the major histocompatibility complex I (MHC I) pathway, leading to the production of the cytotoxic T lymphocytes (CTLs) that specifically kill tumor cells [12]. More and more research substantiates that the tumor vaccines directed towards lymph nodes significantly amplify the immune response [13–16]. Therefore, the targeted delivery of tumor vaccines to lymph nodes and their uptake by APCs are pivotal factors for achieving effective antigen presentation and further triggering potent vaccine effects.

Nonetheless, the distinctive and intricate physiological structure of lymph nodes imposes specific criteria on the hydrodynamic size of vaccines. It has been found that particles exceeding 100 nm tend to become entrapped in the interstitial matrix. Conversely, particles smaller than 10 nm readily access the bloodstream via capillaries. Only those ranging from 10 to 100 nm can access the lymphatic circulation through the aqueous channels between capillaries and capillary lymphatics [17-19]. This facilitates effective vaccine drainage to the lymph nodes. Besides lymph node drainage, a crucial consideration is whether the vaccines reaching the lymph nodes can be promptly engulfed by APCs. Otherwise, the vaccines may pass through the subcapsular sinus to the outer regions of the lymph nodes and exit via efferent lymphatic vessels [20, 21]. Intriguingly, the endocytic behavior of APCs also displays a particle size preference [22]. However, different to the 10-100 nm size range necessary for lymph node drainage, APCs prefer to phagocytose particles within the 100–500 nm size range [23, 24]. Thus, the nanovaccines satisfying the criteria for both lymph node drainage and APC endocytosis hold promising potential. Recently, researchers have endeavored to address the challenges related to the particle size design of lymph node-targeted vaccines. For instance, Wang et al. employed photothermally induced phase-change materials to achieve in-situ alteration of vaccine particle size within the lymph nodes. This simultaneously improved lymph node drainage and APC uptake [25]. Qin et al. used a bioorthogonal reaction to improve vaccine targeting by first delivering a target inside the lymph node by albumin hitchhiking, and then the vaccine could be successfully targeted to the lymph node by an in vivo click reaction [26]. To date, the granularity paradox concerning targeted delivery to lymph nodes and subsequent uptake by APCs persists as a critical challenge in the development of efficient tumor vaccines.

To circumvent the need for intricate synthesis processes or additional therapeutic interventions, we advocate a streamlined approach aimed at concurrently facilitating lymph node drainage and bolstering APCs uptake within the lymph nodes, thereby eliciting a potent tumor-specific cellular immune response. Firstly, we synthesized hollow mesoporous manganese dioxide (MnO₂) nanoparticles with an approximate particle size of about 90 nm through a hard template approach. The substantial specific surface area of these nanoparticles allowed loading of the model tumor antigen ovalbumin (OVA), resulting in the formation of MnO₂/OVA nanoparticles. To boost the uptake by APCs within the lymph nodes, DNA single strands A_{50} and T_{20} adsorbed onto the MnO₂/OVA nanoparticles, yielding MnO₂/OVA/A₅₀ and $MnO_2/OVA/T_{20}$, respectively. Subsequently, both of the nanoparticles were administered sequentially via subcutaneous inoculation by simple time-interval injections. This facilitated the entry of the vaccines into the lymphatic circulation in a state of small particle size. Upon reaching the lymph nodes, MnO₂/OVA/A₅₀ and MnO₂/ OVA/T₂₀ nanoparticles converged and aggregated via the complementary binding between A₅₀ and T₂₀. This aggregation augments the vaccines' particle size and facilitates their uptake by APCs within the lymph nodes. Furthermore, following internalization by APCs, the MnO₂ within the vaccines underwent gradual degradation to Mn²⁺ within the mildly acidic environment of lysosomes, thus serving as an immune adjuvant. The immune response and anti-tumor efficacy of the MnO₂/OVA/ A₅₀-T₂₀ combination vaccine were assessed through in vitro cellular assays, immunization assays, and a melanoma-bearing animal test, respectively. This innovative design strategy, capable of concurrently facilitating lymph node drainage and augmenting APC antigen uptake, can guide the development of efficient lymph node-targeting tumor vaccines.

Materials and methods

Materials

Tetraethyl orthosilicate (TEOS), ethanol, ammonia, potassium permanganate (KMnO₄), and sodium carbonate (Na₂CO₃) were purchased from Macklin (China). Ovalbumin (OVA) was obtained from Sigma (USA). OVA-Cy5.5 was obtained from QIYUE BIOLOGY(China). DNA single strands A_{50} and T_{20} were brought from Tsingke Biotech (China). Enhanced CCK-8 kit, Lyso-Tracker green fluorescent dye, 4',6-diamidino-2-phenylindole (DAPI) and BCA protein assay kit were purchased from Beyotime (China). Roswell Park memorial institute (RPMI) 1640 culture medium, dulbecco's modified eagle medium (DMEM), and fetal bovine serum (FBS) brought from Procell (China). Anti-CD11c-APC, anti-MHC II-PE, anti-MHC I-PE, anti-CD80-Cy5.5, anti-CD86-FITC, FITC-anti-CD4, Cy5.5-anti-CD8a, PE-anti-CD44, APC-anti-CD62L and APC-anti-CD3 antibodies were supplied by BioLegend (USA). Enzyme-linked immunosorbent assay (ELISA) Kits for INF- γ , TNF- α , IL-4, and IL-6 were also purchased from BioLegend (USA). In addition, all animal experiments were determined eligible for the study and were approved by the Ethics Committee of Jinan University.

Synthesis and characterization of MnO₂

The MnO₂ nanoparticles were synthesized by modifying previously published methods [27]. To begin, silica nanoparticles (SiO₂) were synthesized as a hard template using the widely adopted Stöber method. Ethanol (25 mL), deionized water (0.5 mL), and ammonia (1.8 mL) were mixed in a 50 mL flask under uniform stirring. After that, TEOS (0.75 mL) was added into the flask, and the reaction was continued for 24 h at 40 °C. The resulting SiO₂ nanoparticles were collected by centrifugation (10,000 rpm, 20 min) and washed repeatedly. The obtained SiO_2 nanoparticles were dispersed in deionized water (100 mg, 1 mg/ mL). KMnO₄ solution (10 mg/mL, 75 mL) was then added dropwise to the above suspension and stirred for 6 h. The resulting nanoparticles were collected by centrifugation (10,000 rpm, 20 min) and etched with Na_2CO_3 solution (2 M) at 60 °C for 16 h to obtain the MnO₂ nanoparticles. The morphology structures of MnO₂ nanoparticles were observed by the TEM (JEOL TEM-1210, Japan). UV-Vis absorption spectra were measured by a UV-2550 spectrophotometer (SHIMADZU, Japan). FT-IR spectra were recorded by a FT-IR spectrophotometer (VERTEX 70). Size and Zeta potential were detected by the dynamic light scattering (DLS) (Zetasizer Nano ZS, UK).

Preparation of Alum/OVA, MnO_2/OVA, MnO_2/OVA/A_{50} and MnO_2/OVA/T_{20}

The Alum/OVA vaccine was prepared by mixing 0.25 mL aluminum adjuvant with 0.1 mL OVA (3 mg/mL) and diluted with saline into a total volume of 1 mL. The MnO_2/OVA vaccine formulation was prepared by dispersing 1 mg MnO₂ nanoparticles in 0.9 mL saline, adding 0.1 mL OVA (3 mg/mL) solution, and mixing for 4 h. After centrifugation, the free OVA in supernatant was detected with a microplate reader (BIOTEK, USA). Subsequently, 0.5 mL MnO₂/OVA suspension was added to 10 μ L A₅₀ or T₂₀ (100 μ M) and continued stirring for 2 h to obtain MnO₂/OVA/A₅₀ or MnO₂/OVA/T₂₀ vaccine formulation. The morphology structures of the MnO₂/OVA/DNA nanoparticles were observed by the TEM. The UV-Vis absorption spectra of MnO₂, MnO₂/OVA/

 A_{50} , and $MnO_2/OVA/T_{20}$ were measured by a UV-2550 spectrophotometer (SHIMADZU, Japan). The elemental analysis of nanoparticles was detected using an energy dispersive X-ray spectrometry (EDS) in combination with a high angle annular darkfield scanning transmission electron microscopy (HAADF-STEM, JEM 2100 F, Japan).

In vitro cytotoxicity and degradation evaluation

Firstly, DC 2.4 cells were seeded in a 96-well plate at a density of 10^4 cells/well and cultured in an incubator for 24 h. After washing with PBS, the cells were exposed to different concentrations of MnO₂, MnO₂/OVA, MnO₂/OVA/A₅₀, or MnO₂/OVA/T₂₀ (20, 40, 60, 80, 100 µg/mL) for 24 h. Finally, after washing with PBS, 100 µL of 10% CCK-8 reagent was added to each well to detect cell viability.

To evaluate the degradation performance of MnO_2 , DC2.4 cells were seeded in 12-well plates, and then the nano-vaccine (concentration of MnO_2 : 20 µg/mL) was added and co-cultured with the cells for 48 h. Finally, the cells were lysed and centrifuged, and the supernatant was taken to determine the intracellular Mn^{2+} concentration by the ICP.

In vitro antigen uptake and subcellular co-localization experiment

The DC2.4 cells were seeded into a 24-well plate (1×10^5) cells/well) and incubated for 24 h. After washing with PBS, the cells were incubated with free OVA-cy5.5, MnO₂/OVA-cy5.5, MnO₂/OVA-cy5.5/A₅₀, MnO₂/OVAcy5.5/T $_{\rm 20}$, or $MnO_2/OVA\text{-}cy5.5/A_{\rm 50}\text{-}T_{\rm 20}$ (concentration of MnO₂: 20 μ g/mL, OVA: 6 ug/mL, A₅₀/T₂₀: 0.04 μ M) for 6 h. Finally, the cells were digested with trypsin, washed with PBS, and analyzed by flow cytometry. In addition, DC2.4 cells were seeded in cell culture dishes $(5 \times 10^4 \text{ cells/dish})$, and incubated for 24 h. Then, the cells were incubated for 6 h with free OVA-cy5.5, MnO₂/ OVA-cy5.5, MnO₂/OVA-cy5.5/A₅₀, MnO₂/OVA-cy5.5/ T₂₀, or MnO₂/OVA-cy5.5/A₅₀-T₂₀ formulations. Subsequently, the cells were incubated for 2 h with the Lyso-Tracker green fluorescent dye and then fixed for 20 min. Finally, the cells were stained with DAPI dye for 5 min and observed with a confocal laser scanning microscope (CLSM, Zeiss, Germany).

Detection of lysosome integrity

The DC2.4 cells were seeded and incubated in 24-well plates (5×10^4 cells/well) for 24 h. Next, the cells were stained for 1 h with 5 µg/mL acridine orange dye solution. After removing the dye, the cells were cultured for 24 h with OVA, MnO₂/OVA, MnO₂/OVA/A₅₀, MnO₂/OVA/A₅₀, MnO₂/OVA/A₅₀, T₂₀, or MnO₂/OVA/A₅₀-T₂₀ formulations. The

distribution of acridine orange in the cells was observed with a fluorescence microscope (DMRA2, Leica, Germany).

In vitro maturation and cross-presentation tests of BMDCs

The Bone marrow-derived dendritic cells (BMDCs) were obtained using a previously reported method [28]. In brief, the bone marrow cells were obtained from the tibia and femur of C57BL/6 mice (4–6 weeks) under aseptic conditions. The remaining cells were collected after lysis of red blood cells with red blood cell lysis buffer and cultured in RPMI 1640 complete medium containing 10% FBS, 1% penicillin/streptomycin, GM-CSF (20 ng/mL), and IL-4 (10 ng/mL). The medium was replaced with half fresh medium every two days, and the cells were harvested on the sixth day for subsequent experiments.

To assess the effect of vaccine formulations on enhancing antigen cross-presentation and DC activation, BMDCs were seeded in low-adhesion 24-well plates at a density of 5×10^5 cells/well. Then, the cells were cocultured with free OVA, MnO₂/OVA, MnO₂/OVA/A₅₀, and MnO₂/OVA/T₂₀ or MnO₂/OVA/A₅₀-T₂₀ (OVA: 5 µg/ well) for 24 h. Finally, BMDCs were collected and stained with anti-CD11c-APC, anti-MHC II-PE, anti-MHC I-PE, anti-CD80-Cy5.5, and anti-CD86-FITC, and then quantitatively analyzed using a flow cytometer. Further, in order to verify the mechanism by which MnO₂ promotes DC maturation, we measured the level of INF- β secreted by BMDC in the presence of manganese dioxide by using an mINF- β 2.0 assay kit (InvivoGen, USA).

In vivo evaluations of LNs targeting

To determine the optimal time for materials to reach LNs, C57BL/6 mice (6-8 weeks) were selected for subcutaneous injection of MnO₂/OVA-Cy5.5 (n=3). At 2, 6, 12, 24, and 48 h after injection, inguinal LNs near the injection site were subsequently collected and imaged ex vivo using a small animal bioluminescence imaging system (IVIS Lumina III, PerkinElmer, USA). To verify the better LNs retention ability of the MnO₂/OVA-cy5.5/ A_{50} - T_{20} , C57BL/6 mice (6–8 weeks) were subcutaneously injected with 50 µL Saline, OVA-Cy5.5, MnO₂/OVA-Cy5.5, MnO₂/OVA-Cy5.5/A₅₀, MnO₂/OVA-Cy5.5/T₂₀, and MnO₂/OVA-Cy5.5/A₅₀, respectively. After 24 h, 50 µL Saline, OVA-Cy5.5, MnO₂/OVA-Cy5.5, MnO₂/OVA-Cy5.5/A₅₀, MnO₂/OVA-Cy5.5/T₂₀, and MnO₂/OVA- $Cy5.5/T_{20}$ were injected again in same site. Inguinal LNs near the injection site were collected 24 h later for ex vivo IVIS imaging which was performed by an IVIS Lumina XR equipment (IVIS Lumina III, USA).

Immunization and immune responses

The female 6–8 weeks C57BL/6 mice were randomly divided into seven groups (n=6) and subcutaneously

injected with OVA, Alum/OVA, MnO_2/OVA , MnO_2/OVA , $MnO_2/OVA/A_{50}$, $MnO_2/OVA/T_{20}$, and $MnO_2/OVA/A_{50}$ - T_{20} on days 0, 1, 7, 8, 14, and 15, respectively. On day 21, the spleens were collected to prepare splenocyte suspension for subsequent detection.

Flow cytometry was used to quantitatively analyze DC maturation and T cell differentiation in the spleen of different groups of mice. Direct staining of splenocytes with anti-CD11c-FITC, anti-MHC I-PE, anti-CD86-Cy5.5, and anti-CD80-APC was used to observe the maturation of DCs in splenocytes, and the efficiency of cross-presentation of antigen. Splenocytes were stained with anti-CD3-APC, anti-CD8a-Cy5.5, and anti-CD4-FITC to determine the proportion of CD4⁺ and CD8⁺ T cells in splenocytes. To visualize the proportion of memory T cells in splenocytes, splenocytes were directly stained with FITC-anti-CD4, PerCP-Cy5.5-anti-CD8a, PE-anti-CD44, and APC-anti-CD62L, and then detected by the flow cytometer which carried out on a Beckman Cyto-FLEX flow cytometry (USA).

In vivo antitumor efficacy

C57BL/6 mice (6-8weeks) were randomly divided into six groups (n=6) and inoculated with B16-OVA cells $(6 \times 10^{6} \text{ cells/mouse})$ on the back of the mice, and subsequently injected with each vaccine when the tumor size was approximately 50 mm³, which was marked as day 0. The mice were injected with a vaccine formulation (OVA: 15 µg) on days 0, 1, 5, 6, 10, and 11. The body weight and tumor volume were monitored at one-day intervals. The tumor volume was calculated using the formula: V= $(L \times W^2)/2$ (where V is the tumor volume, L is the length of the tumor, and W is the width of the tumor). On day 15, the tumors, serum, LNs, spleen, and other major organs (heart, liver, lung, and kidney) were collected for further analysis. The tumor slices were stained with hematoxylineosin (H&E), TUNEL, Ki67, and CD8⁺ dye solutions, and observed with the fluorescence microscope. In addition, the spleens and lymph nodes were collected to prepare splenocyte and lymphocyte suspensions, respectively. The splenocytes and lymphocytes were then stained with anti-CD3-APC, anti-CD8a-Cy5.5, and anti-CD4-FITC to determine the proportion of CD4⁺ and CD8⁺ T cells. The flow cytometry was carried out on a Beckman CytoFLEX flow cytometry (USA).

Statistical analysis

All results are presented as the mean±S.D. from at least three independent experiments. Statistical differences between two groups were determined by Student's t-test, and the differences among three or more groups were determined by one-way or two-way NOVA with the Bonferroni multiple comparison post-test. P values of *p < 0.05, **p < 0.01, ***p < 0.001, and ****p < 0.001 were

regarded as significant differences. Animal survival rates were compared with the log-rank test using GraphPad Prism 9.5.

Results and discussion

Preparation and characterization of MnO₂/OVA/DNA

Hollow manganese dioxide was synthesized by the method previously reported in the literature with a mirror change [27]. As shown in the TEM image (Fig. 1a), MnO_2 showed a uniform spherical morphology with an average particle size of around 90 nm, and the shell thickness of MnO_2 was uniform at about 14.3 nm. As anticipated, manganese elements were shown in the Xray photoelectron spectroscopy (XPS) spectrum (Fig. 1b), the characteristic peaks at 654.2 and 642.4 eV corresponded to the Mn (IV) $2p_{2/3}$ and Mn (IV) $2p_{1/2}$ spin–orbit peaks of MnO_2 , indicating that MnO_2 nanoparticles have been successfully synthesized [29, 30].

The results of the BCA kit assay showed that the OVA loading of MnO2 could reach 300 µg/mg within 4 h (Fig. 1c). For the loading of two different DNA single strands, the supernatants of DNA single strands $(A_{50} \text{ and } T_{20})$ before and after loading by MnO₂/OVA nanoparticles were examined by UV-Vis spectroscopy, as shown in Fig. 1d. The characteristic absorption peaks of A₅₀ and T₂₀ in the supernatants disappeared after loading by MnO₂/OVA nanoparticles, which indicated that the MnO₂/OVA nanoparticles successfully loaded with DNA single strands. The morphologies of MnO₂/OVA/ DNA was shown in Supporting Information Figure S1a, and it can be seen that they are not significantly different from MnO₂. In addition, FT-IR analysis showed (Fig. 1e) that MnO_2/OVA , $MnO_2/OVA/A_{50}$, and $MnO_2/OVA/T_{20}$ showed characteristic peaks at 1645 cm⁻¹ and 1524 cm⁻¹ attributed to amide bonds, indicating the successful loading of OVA [31]. The characteristic peaks of $MnO_2/OVA/$ A_{50} and $MnO_2/OVA/T_{20}$ at 1067 cm⁻¹ were attributed to phosphate groups, indicating the successful loading of DNA single chains [32]. Subsequently, UV-Vis spectra were recorded to distinguish the different products from material synthesis to vaccine preparation (Fig. 1f), MnO₂ showed broad spectrum absorption at 200-600 nm. In contrast, vaccine formulation loaded with OVA and DNA single strands caused a different degree of red shift in the position of the maximum absorption peak of MnO_2 . The zeta potentials of the intermediates (Fig. 1g) of the vaccine formulations all changed significantly, indicating that the modification and loading at each step of the vaccine formulations process were successful.

To test if $MnO_2/OVA/A_{50}$ and $MnO_2/OVA/T_{20}$ could achieve base-pairing-triggered aggregation, we demonstrate the occurrence of nanoparticle aggregation phenomena after a simple mixing of the two groups of materials through TEM images (Fig. 1h), which shows that the vaccine aggregates formation. The DLS further demonstrated the change in particle size which the size increased from 91.0 to 91.3 nm to 396 nm after simple mixing (Fig. 1i). Notably, the size measured by DLS is much larger than that measured by TEM, which may be attributed to the different imaging conditions as the measurement of TEM was conducted under a dry state, while DLS measurements were in fully hydrated states [33]. The results together demonstrated that MnO₂/OVA/A₅₀ and MnO₂/OVA/T₂₀ could rapidly form aggregation with simple mixing. In addition, the results of the elemental analyses showed that MnO₂/OVA/A₅₀ and MnO₂/OVA/ T_{20} aggregated into large size particles containing the Mn, N, O, and P elements (Fig. 1j). Together, these results confirm that $MnO_2/OVA/A_{50}$ and $MnO_2/OVA/T_{20}$ could aggregate in response to A_{50} and T_{20} base pair pairing.

In vitro assessment of cytotoxicity, cellular uptake, and antigen lysosome escape

An initial assessment of the biocompatibility of the vaccine is required before a comprehensive evaluation of the vaccine through various cellular and animal assays. After treating the cells with different concentrations of MnO_2 , MnO_2/OVA , $MnO_2/OVA/A_{50}$, and $MnO_2/OVA/T_{20}$ for 24 h, the cell viability was detected by using the CCK-8 kit. As shown in Supporting Information Figure S1b and Fig. 2a, MnO_2 exhibited slight cytotoxicity within a certain range, but the loading of OVA and DNA strands could effectively enhance the biosafety of the vaccine. Finally, 20 µg/mL was chosen as the optimal dose of $MnO_2/OVA/DNA$ for subsequent in vitro experiments. These results of the in vitro cytotoxicity experiments showed that the nanovaccines prepared in this study have good biosafety and can be used for further bioassays.

The effective endocytosis of nanovaccines by antigenpresenting cells plays a decisive role in activating the adaptive immune response. Therefore, Cy5.5-labeled OVA antigen was used to explore the endocytosis efficiency of different nanovaccines. The DCs were subsequently co-incubated with different vaccine groups for 6 h and the distribution of antigen in the cells was observed by CLSM. As shown in Fig. 2b, the green and red signals represented lysosomes and OVA, respectively. Due to the low uptake of free OVA by the cells, the red fluorescent signal was weaker in the OVA group and the green signal almost overlapped with the red signal, indicating that OVA failed to be released from the lysosomes into the cytoplasm. In contrast, the red fluorescence signal was significantly enhanced in the MnO₂-containing groups, and antigen lysosome escape was also observed. This indicated that biodegradable MnO₂ can successfully deliver antigens to the cytoplasm. Notably, the red fluorescence signal in the A-T base pair pairing group (MnO₂/OVA-cy5.5/A₅₀-T₂₀) was the strongest and was



Fig. 1 Characterizations of synthesized vaccine. **a**) TEM image of MnO_2 nanoparticles. Scar bar: 500 nm. **b**) XPS analysis of MnO_2 nanoparticles. **c**) The capacity of OVA by MnO_2 nanoparticles. **d**) Changes in DNA absorption peaks in the supernatant before and after loading the MnO_2/OVA with DNA. **e**) FT-IR spectra of different samples. **f**) UV-vis absorption spectra of different samples. **g**) Zeta potentials of the intermediate products during the preparation process of nanovaccines. **h**) TEM images of $MnO_2/OVA/A_{50}$ and $MnO_2/OVA/T_{20}$ after mixing. **i**) The size curve of $MnO_2/OVA / A_{50}$ and $MnO_2/OVA/T_{20}$ before and after mixing. **j**) HAADF-STEM images of $MnO_2/OVA / A_{50} - T_{20}$

found to be significantly less co-localized with the lysosomes by fluorescence intensity paving. This corroborates that the A-T base pair pairing group has higher antigen endocytosis efficiency and stronger lysosomal escape ability. In addition, as shown in Fig. 2c-d, the endocytosis efficiency of all vaccine formulations with MnO_2 as the carrier was significantly higher than that of the free OVA group, while the endocytosis efficiency of the A-T base pair pairing group also separated significantly from the other MnO_2 carrier groups, indicating that due to the increased particle size in the A-T base pair pairing group, it was able to be more effectively taken up by DC cells, thus may promote the adaptive immune response [25].

By evaluating the degradation behavior of the vaccine in the cell, it was found that the vaccine could reach 10% degradation rate at 48 h after cellular uptake, which provides the possibility for the vaccine to achieve lysosomal escape (Supporting Information Figure S1c). We speculate that MnO_2 decomposes to Mn^{2+} in the micro acidic environment within the lysosome, which may lead to an increase in lysosomal osmotic pressure, disrupting the lysosome and thus promoting antigen cross-presentation. Acridine orange, a hetero-staining fluorescent dye, exhibits red fluorescence in lysosomal species and green fluorescence in the cytoplasm and can be used to detect lysosomal integrity. When the lysosomal membrane is disrupted, the intensity of red fluorescence decreases [34]. As shown in Fig. 2e, free OVA had little effect on the lysosomes, which are structurally intact and show more orange fluorescence under fluorescence microscopy. In contrast, the MnO₂-containing group showed different degrees of diminished red fluorescence, which indicated



Fig. 2 In vitro cellular assays of various vaccine formulations. **a**) Cytotoxicity assessment of $MnO_2/OVA/A_{50}$ and $MnO_2/OVA/T_{20}$ incubated with DC2.4 cells for 24 h and measured by the CCK-8 assay kit. **b**) CLSM images of DC2.4 cells after incubation with different vaccine formulations for 6 h. OVA, lyso-some, and cell nucleus were respectively labeled with Cy5.5 (red), LysoTracker FITC (green), and DAPI (blue). Rr is the Pearson correlation coefficient for fluorescence co-localization of lysosomes with OVA (analyzed by ImageJ). The scale bar represents 10 µm. **c**) Corresponding mean fluorescence intensity of every group in the cellular uptake assay. **d**) Representative flow cytometry histograms for OVA uptake efficiencies of DC2.4 cells in various groups. **e**) Lysosomal integrity observation of DC 2.4 cells exposed to vaccine preparations for 24 h, and semi-quantitative analysis of fluorescence (analyzed by Image J). The significance was analyzed using a one-way analysis of variance (ANOVA). *p < 0.05, **p < 0.01, ***p < 0.001, ***p < 0.001

that the structural integrity of the lysosomes might be damaged to different degrees. Among them, the red fluorescence in the A-T base pair pairing group ($MnO_2/OVA/A_{50}-T_{20}$) was most obviously diminished, and the superimposed fluorescence photos showed yellow-green fluorescence, indicating that this group had the greatest lysosomal damage. The semi-quantitative fluorescence analysis of the photographs also showed the same trend. This may be because of the greater uptake of MnO_2 by APCs in the A-T base pair pairing group, resulting in greater release of Mn^{2+} , which promotes lysosomal rupture and antigen lysosome escape.

In vitro evaluation of activation and antigen crosspresentation of BMDCs

DCs are the most potent antigen-presenting cells known, capable of efficient uptake, processing, and presentation of antigens. Immature DCs become mature DCs after capturing antigens, expressing co-stimulatory molecules such as CD80, CD86, etc. When antigen escapes from the lysosome to the cytoplasm, facilitating its delivery to CD8⁺ T cells via the MHC I pathway to produce CTL, i.e., antigen cross-presentation. To demonstrate that the vaccine stimulates DC maturation and promotes antigen cross-presentation, BMDCs were extracted from mice and co-cultured with the vaccine formulations for 24 h. Then, the expression of OVA-specific MHC I,

MHC II, CD80, and CD86 molecules of BMDCs were analyzed, and the results were shown in Fig. 3 and Supporting Information Figure S3 (flow cytometry gating strategy was shown in Supporting Information Figure S2). Compared with the OVA group compared with the OVA group, the MnO₂-containing group exhibited significant upregulation of MHC II (Supporting Information Figure S3a & Fig. 3a), and compared with the Alum/OVA group, the MnO₂-containing group exhibited significant upregulation of CD80 and CD86 molecules (Fig. 3b and e) and CD40 molecules (Supporting Information Fig. 3c & Figure S3b), which indicated that MnO₂ effectively stimulated the maturation of BMDCs and promoted the antigen presentation. Notably, the A-T base pair pairing group showed the highest expression of MHC I molecules (Fig. 3d and f), which was consistent with the previous results of cellular endocytosis and antigen lysosome escape experiments, suggesting that A_{50} and T_{20} pairing promotes vaccine aggregation to elicit stronger antigen cross-presentation based on its higher endocytosis efficiency. Manganese is a nutritious inorganic trace element required for a variety of physiological processes. Jiang et al. [35, 36] found that Mn^{2+} in the cytoplasm can play an alarming role, activate the cGAS-STING cascade, promote the production of large amounts of interferon type I, and enhance the activation of DC and the crosspresentation reaction of antigens. Therefore, we further



Fig. 3 Nanovaccines efficiently activate BMDCs in vitro. The expression of **a**) MHC II, **b**) CD80 and CD86, **c**) CD40, and **d**) MHC I in CD11c⁺ BMDCs. Representative flow cytometry dot plots of **e**) DCs maturation and **f**) MHC I expressed on CD11c⁺ BMDCs in various groups (gated on CD11c⁺ cells). The representative plot dots of MHC II and CD 40 were shown in Figure S2. Error bars represent \pm SD (n=3). The significance was analyzed using one-way analysis of variance (ANOVA). *p < 0.05, **p < 0.001, ***p < 0.001, ***p < 0.001

examined the concentration of type I interferon IFN- β in the DC supernatant after incubation with MnO₂ nanovaccines, and the results are shown in Supporting Information Figure S4. MnO₂ increased the Mn²⁺ content in the cytoplasm, and significantly increased the concentration of IFN- β in the DC supernatant, which is an important reason for the enhancement of DC maturation.

In vivo LNs targeted delivery

For passive LNs targeting vaccines, the LNs drainage capacity and LNs retention capacity of the vaccine are most critical. Next, the LN's targeting ability of the vaccine was examined using the IVIS imaging system. Considering that factors affecting lymph node drainage (size, shape and zeta potential) were not significantly different between MnO₂/OVA and MnO₂/OVA/DNA nanoparticles, the MnO₂/OVA-Cy5.5 vaccines were selected as the study subject and injected subcutaneously into the right and left groin of C57BL/6 mice. The mice were then performed live imaging at 2, 6, 12, 24, and 48 h, after which the inguinal LNs were isolated for fluorescence imaging to observe the accumulation of fluorescence at the LN sites. As shown in Fig. 4a, the fluorescence at the injection site gradually decreased with time and disappeared at 24 h, indicating that the vaccine gradually migrated passively, possibly to the LNs. Therefore, the LNs were isolated from the mice and their fluorescence intensity was observed at each time point. As shown in Figure b-c, the fluorescence of the LN was strongest at 2 h after injection, indicating that the vaccine reached the highest amount of LN at this time. Subsequently, the fluorescence intensity of the LNs began to diminish with time. This corroborates the view reported in the literature that due to the weak retention capacity of LNs, the conventional materials enter the LNs merely by passing through, and cannot be effectively endocytosed by APCs.

Next, for LNs-targeted vaccines administered in two doses, the timing of the second dose is critical for vaccine efficacy. Based on the results of LNs ex vivo imaging, an interval of 2 h should have been chosen as the time of the second vaccination. However, considering that a large amount of the first dose of vaccine was still left at the injection site, the second dose of vaccine at this time might cause the vaccine to accumulate at the injection site and affect the efficiency of its LN drainage. Therefore, we chose 24 h as the time interval for the second vaccine injection and took this as the standard for the complete two vaccine doses in this study (Supporting Information Figure S5). The inguinal LNs were removed for fluorescence imaging 24 h after the second vaccine dose, as shown in Fig. 4d-e. The fluorescence signals in the LNs of the conventional vaccine group in which the nanovaccines could not accumulate in the LNs were at a similar and lower level. The A-T base pair pairing group $(MnO_2/OVA-cy5.5/A_{50}-T_{20})$, on the other hand, showed strong fluorescence, indicating that the $MnO_2/OVA-cy5.5/A_{50}-T_{20}$ group had a stronger capacity to detain in LNs. In addition, no significant differences were found in the accumulation of vaccines in the livers and spleens (Supporting Information Figure S6). Taken together, the experimental results showed that the 1st particle dose can still be compounded with 2ed particle dose, increasing the size of the nanovaccines in the LNs and significantly increasing the amount of vaccine accumulation within the lymph nodes which indicates the strategy of inducing vaccine aggregation in LNs through A-T base pair pairing to enhance vaccine uptake by APCs has achieved preliminary success.

Enhanced in vivo cellular immune responses

Encouraged by the results of the above in vitro and in vivo experiments, the ability of different nanovaccines to induce an antigen-specific immune response was further evaluated with the vaccination regimen shown in Fig. 5a. As mentioned earlier, DC activation is an important step to activate the natural immune response. After three immunizations against C57BL/6 mice, the activation level of DCs in the collected spleen was examined. As shown in Fig. 5b-g and Supporting Information Figure S8 (flow cytometry gating strategy was shown in Supporting Information Figure S7), the expressions of MHC II, CD80, CD86, and CD40 molecules were significantly promoted by the A-T base pair pairing group (MnO₂/OVA/ A_{50} - T_{20}) compared with OVA group, indicating that the MnO₂/OVA/A₅₀-T₂₀ vaccine formulation significantly enhanced the maturation of DCs in vivo and induced more effective antigen delivery and immune response in immunized mice. Moreover, compared with the OVA group, the MHC I expression was significantly enhanced in the $MnO_2/OVA/A_{50}\mbox{-}T_{20}$ group (Fig. 5d&f), which also verified that the MnO2/OVA/A50-T20 group had the highest cross-presentation efficiency, which could be attributed to the aggregation of nanoparticles after base pairing, increasing the chances for DCs to capture antigens and facilitate their delivery into the cytoplasm. The co-stimulatory molecule CD40 effectively promoted the formation of immune synapses between APCs and T cells, which in turn activated T cells, as shown in Fig. 5e. CD40 signaling is an important trigger for the monocyte maturation process, and binding of CD40 to the DCs surface promotes the production of cytokines and chemokines, induces the expression of co-stimulatory molecules, and facilitates antigen cross-presentation [37]. The expression of CD40 was much higher in the MnO₂/OVA/ A_{50} - T_{20} group than in the MnO₂/OVA and MnO₂/OVA/ A₅₀ groups, which again suggests that A-T base pair pairing induced nanoparticle aggregation and then induced stronger body immunity. As shown in Fig. 6a&b, DCs



Fig. 4 In vivo systemic distribution of nanovaccines. **A**) In vivo fluorescence imaging of mice at different times (2, 6, 12, 24, and 48 h) after subcutaneously injected MnO₂/OVA (100 μ L per mouse). OVA was labeled with Cy5.5. **b**) IVIS fluorescence imaging of the isolated inguinal LNs from C57BL/6 mice (*n* = 3) at different time points after MnO₂/OVA (100 μ L per mouse) administration. **c**) Quantification of the accumulated fluorescence in LNs over time. **d**) IVIS images and **e**) quantification of the fluorescence in LNs from the mice (*n* = 3) injected with saline, free OVA, MnO₂/OVA, MnO₂/OVA/A₅₀, MnO₂/OVA/T₂₀, or MnO₂/OVA /A₅₀. T₂₀. Error bars represent ± SD (*n* = 3). The significance was analyzed using a one-way analysis of variance (ANOVA). **p* < 0.05, ***p* < 0.01, *****p* < 0.001

activated by the $MnO_2/OVA/A_{50}$ - T_{20} group vaccine formulation significantly increased the proportion of CD8⁺ T cells, implying that the vaccine effectively stimulated the proliferation and differentiation of T cells, suggesting its potential application as a therapeutic tumor vaccine for tumor immunotherapy.

In vivo evaluation of the immune memory effect

The main function of vaccines in the natural immune system is to induce antigen-specific immune memory so that the immune system can respond rapidly when it is invaded by the same antigen. In this process, memory T cells are the key to generate effective immune memory in the body. Usually, memory T cells are divided into effector memory T cells (T_{EM}, CD44^{high}CD62L^{low}) and central memory T cells (T_{CM}, CD44^{high}CD62L^{high}) according to the cell surface receptors. Among them, T_{CM} can proliferate and differentiate into T_{EM} in response to antigen stimulation, while CD4⁺ T_{EM} can activate the immune system by inducing cytokine secretion such as INF- γ , and CD8⁺ T_{EM} can directly recognize and kill tumor cells. As shown in Fig. 6c-d and e-f, the MnO₂/OVA/A₅₀-T₂₀ group was able to significantly induce a higher proportion of CD4⁺ T_{EM} and CD8⁺ T_{EM} compared to the



Fig. 5 The evaluation of immune response after C57BL/6 mice were immunized with various vaccine formulations three times. Schematic illustration of the process of s. c. injection of nano-vaccines in preventive immune mode. **b**-**e**) Percentage of **b**) MHC II, **c**) DCs maturation, d) MHC I, **e**) CD40 expressed on CD11c⁺. Representative flow cytometry plots of f) MHC II and **g**) MHC I in spleen harvested from immunized mice. The representative plot dots of DC maturation and CD40 were shown in Figure S5. Error bars represent \pm SD (n=6). The significance was analyzed using a one-way analysis of variance (ANOVA). *p < 0.05, **p < 0.01, ***p < 0.001



Fig. 6 The assessment of immune memory effects after the mice were immunized with various vaccine formulations three times. **a**) Representative flow cytometry dot plots of CTLs (gated on CD3⁺ T cells) in the various groups. **b**) the ratio of CD8⁺/CD4⁺ T cells in CD3⁺ T cells. **c**) Representative flow cytometry results of effector memory T cells, gated on CD4⁺. **d**) The frequencies of effector (CD44^{hi}CD62L^{low}) memory CD4⁺ T cells in the splenocytes. **e**) Representative flow cytometry results of effector memory T cells, gated on CD8⁺ T cells. **f**) The frequencies of effector (CD44^{hi}CD62L^{low}) memory CD4⁺ T cells in the splenocytes. **e**) reells in the splenocytes. Error bars represent ± SD (n=6). The significance was analyzed using a one-way analysis of variance (ANOVA). *p < 0.05, **p < 0.01, ***p < 0.001

other vaccine formulation groups, which further demonstrated that the $MnO_2/OVA/A_{50}$ - T_{20} vaccine formulation induced more significant immune memory effects, indicating its potential role in tumor prevention that specifically kills target cells without destroying normal cells.

In vivo antitumor efficacy

To investigate the anti-tumor ability of those nanovaccines, we performed an in vivo anti-tumor assessment using the B16-OVA melanoma model. As shown in Fig. 7a, B16-OVA cells were injected subcutaneously in C57BL/6 mice, and after 7 days they were divided into six groups and inoculated subcutaneously with various agents on days 0, 1, 5, 6, 10, and 11. Tumor volumes were measured every other day during the treatment period, as shown in Fig. 7b and Supporting Information Figure S9. The average and individual tumor growth curves showed that the B16-OVA tumors grew rapidly in saline and OVA groups, and the nanovaccines significantly inhibited the tumor growth, with the most excellent tumor inhibition in the MnO₂/OVA/A₅₀-T₂₀ group. Supporting Information Figure S10 showed that all groups of mice showed a slight increase in body weight with time. Tumor volume up to 1500 mm³ was used as the survival criterion, and only the survival rate of mice in the MnO₂/ OVA/A₅₀-T₂₀ group was maintained at 100% until the end of the antitumor experiments (Fig. 7c). Similarly, the tumor weight in the MnO₂/OVA/A₅₀-T₂₀ group was slighter, which also confirmed that the MnO₂/OVA/ A_{50} - T_{20} group had the best anti-tumor effect (Fig. 7d). Hematoxylin-eosin (H&E) staining of the tumor tissues showed that the tumors in the MnO₂/OVA/A₅₀-T₂₀ group showed extensive necrosis, whereas the tumors in the other groups remained more viable (Fig. 7e). The





Fig. 7 In vivo inhibition of melanoma tumors by treatment with nanovaccines. **a**) The schematic illustration of the tumor therapy experiment. **b**) Tumor growth curves of B16-OVA-tumor-bearing mice after various treatments. **c**) Tumor weights with various treatments collected on day 15. **d**) Mice survival time results. **e**) H&E images of tumor tissues collected on day 15 after various treatments. Immunofluorescence staining of **f**) Ki67 and **g**) Tunnel in the tumors. Error bars represent \pm SD (n=5). The significance was analyzed using a one-way analysis of variance (ANOVA). *p < 0.05, **p < 0.01, ****p < 0.001

immunofluorescence images of TUNEL (apoptosis) and Ki67 (cell proliferation), as illustrated in Fig. 7f and g, respectively, demonstrated that the MnO₂/OVA/A₅₀-T₂₀ vaccine formulation induced more pronounced apoptosis and a larger area of damage than the other vaccine formulations under identical conditions [13]. Moreover, the extent of cell proliferation in the MnO₂/OVA/A₅₀-T₂₀ group was significantly diminished, collectively indicating the favorable anti-tumor efficacy of the MnO₂/OVA/A₅₀-T₂₀ vaccine formulation.

To investigate the in vivo immune response of the B16-OVA melanoma model, the inguinal LNs were collected from mice in different vaccine formulation groups, as shown in Supporting Information Figure S11. The volume of LNs in the DNA-containing vaccine formulation groups was significantly increased compared with MnO_2/OVA groups, among which, the volume of LNs in the $MnO_2/OVA/A_{50}$ -T₂₀ group was the largest. These results suggested that a stronger immune response induced lymphocyte proliferation in the mice treated with the $MnO_2/OVA/A_{50}$ -T₂₀ group was the largest.

 OVA/A_{50} - T_{20} group. CTLs, as the anti-tumor mainstay of the initial T cells differentiated after cellular immunity was activated. Here, single-cell suspensions of LNs and spleens were obtained by grinding, and the proportions of CTLs in the LNs and spleens were analyzed. As shown in Fig. 8a and c, the cytotoxic CD8⁺ T cells were significantly increased in the LNs of the mice treated with the MnO₂/OVA/A₅₀-T₂₀ group. Their proportions in sple-

nocytes were further explored as shown in Fig. 8b and d,

compared with the saline group, the percentage of CD8⁺

T cells in the splenocytes of mice treated with the DNA-

containing group was significantly higher, and the highest CD8⁺ T cells were found in the $MnO_2/OVA/A_{50}-T_{20}$

group, which indicated that MnO₂ as an adjuvant and

nanoparticle aggregation due to A-T base pair pairing

indeed assist in the activation of organismal immunity,

especially the cellular immune response. T-lymphocyte

infiltration in tumor tissues was equally important for

tumor cell killing. The immunofluorescence staining of

tumor tissue sections was then performed as shown in



Fig. 8 In vivo antitumor immunotherapeutic study. Representative flow cytometry results of **a**) CD3⁺CD8⁺T cells in the lymph nodes and **b**) CD3⁺CD8⁺T cells in the spleens. **c**) The proportion of CD3⁺CD8⁺T cells in the lymph nodes determined by flow cytometry. **d**) The proportion of CD3⁺CD8⁺T cells in the spleen determined by flow cytometry. **e**) Immunofluorescence staining of CD8⁺T cells in the tumors. Error bars represent \pm SD (n = 5). The significance was analyzed using a one-way analysis of variance (ANOVA). *p < 0.05, **p < 0.01, ***p < 0.001, ***p < 0.001

Fig. 8e. The distribution of CD8⁺ T cells was significantly increased in the tumors treated with the MnO₂/OVA/ A_{50} -T₂₀ group, which indicated that this vaccine formulation promoted CD8⁺ T cell infiltration of tumors and significantly exerted an anti-tumor immune response.

Subsequently, the collected splenocytes of the immunised mouse were further co-cultured with B16-OVA cells in vitro for 24 h, as shown in Fig. 9a. A large number of splenocytes in the MnO₂-containing group were attached to the B16-OVA, and the splenocyte clusters of the MnO₂/OVA/A₅₀-T₂₀ group were most obviously attached to tumor cells, which may be that the CD8⁺ T cells in the splenocytes exerted a specific toxicity to B16-OVA [38]. This also proves that the number of CD8⁺ T cells in splenocytes was the highest in the MnO₂/OVA/ A₅₀-T₂₀ group. In addition, the supernatants of splenocytes after co-stimulation with OVA antigen were collected for cytokine secretion level assays. As shown in Fig. 9b-e, compared with the saline group, the secretion of IL-6 cytokine was significantly increased in the MnO₂-containing groups, and that was the highest in the MnO₂/OVA/A₅₀-T₂₀ group. Meanwhile, compared with the saline and OVA group, the secretion of IL-4, IL-6, TNF- α , and INF- γ cytokines was significantly increased in the MnO₂/OVA/A₅₀-T₂₀ group. These results indicated that MnO₂ acted as an adjuvant and could be induced aggregation by A-T base pair pairing at LNs, which promoted the secretion of anti-tumor cytokines and induced stronger immunity. As one of the key indicators of humoral and cellular immune levels, OVA-specific antibody titers were also examined by ELISA, and the results were shown in Fig. 9f-h. compared to the saline and OVA groups, the levels of activated IgG, IgG1, and IgG2a antibody titers in the MnO₂/OVA/A₅₀-T₂₀ group were significantly increased, which suggested that antigen-loaded MnO₂ could effectively promote antibody production,



Fig. 9 a) Photographs of tumor cell-specific killing studies. Scale bars: 250 μm. The serum nanovaccines-specific. b) Secreted levels of IL-4, c) IL-6, d) TNF-α, and e) INF-γ form splenocytes after co-culture with OVA. f) IgG, g) IgG1, and h) IgG2a titers on Day 15. Error bars represent ± SD (*n* = 5). The significance was analyzed using a one-way analysis of variance (ANOVA). **p* < 0.05, ***p* < 0.001, ****p* < 0.001

and the vaccine further enhanced the production of cellular immunity-associated antibody after aggregation in LNs by base-pairing.

Considering the importance of biosafety for vaccines, major organs were collected from the mice vaccinated three times with different vaccine formulations. Major organs such as the heart, liver, spleen, lung, and kidney were observed under the microscope after H&E staining. As shown in Supporting Information Figure S12, no obvious abnormalities and lesions were observed in these organs of all groups, which indicated that the vaccine formulations prepared in the present study did not damage the organs and were sufficiently biologically safe.

Conclusion

In conclusion, this study developed a size-adjustable vaccine delivery system based on the principle of base complementary pairing. This system was designed for targeted delivery to the LNs and to enhance the efficient uptake of antigens by APCs in LNs, thereby improving antigen delivery efficiency. Optimizing the nanoscale particle size of MnO₂/OVA/A₅₀ and MnO₂/OVA/T₂₀ (smaller than 100 nm), which could efficiently deliver them to the LNs. This optimization also induced the formation of nanoparticle aggregates within the LNs through DNA single-strand complementation, thereby increasing the retention time of vaccines in the LNs and facilitating the internalization of vaccines by APCs. These processes lead to effective APC activation, antigen crosspresentation, and a robust immune response in vivo, resulting in excellent anti-tumor effects. This study demonstrates that our vaccine inherits the advantages of traditional LNs-targeted vaccines while addressing potential drawbacks, such as insufficient internalization of the vaccine by APCs within the LNs. This work provides a validated strategy for targeting LNs and introduces innovative ideas for the development of more effective LNstargeted vaccines.

Supplementary Information

The online version contains supplementary material available at https://doi. org/10.1186/s12951-024-02498-1.

Supplementary Material 1

Acknowledgements

Authors thank the Centric Laboratory of Medical College of Jinan University and the Department of Biomedical Engineering of Jinan University for providing experimental and instrument platforms.

Author contributions

Y.Z.: Methodology, Investigation, Data curation, Administration, Software, Writing-original draft. L.F.: Formal analysis, Investigation, Data curation. Z.L.: Conceptualization, Supervision, Resources, Funding acquisition. J.L.: Resources, Conceptualization, Funding acquisition. L.H.: Writing - review & editing, Project administration, Supervision, Resources. All authors reviewed the manuscript.

Funding

This work was financially supported by the Science and Technology Program of Guangzhou, China (No.202103030004), National Natural Science Foundation of China (No.82374306), Natural Science Foundation of Hunan Province (No. 2023JJ30456), Guangdong Basic and Applied Basic Research Foundation (No.2022A1515012148 & 2023A1515011221).

Data availability

No datasets were generated or analysed during the current study.

Declarations

Ethics approval and consent to participate

The animal experiments were approved by The Ethics Committees of Jinan University.

Consent for publication

All authors read and agreed to submit the manuscript.

Competing interests

The authors declare no competing interests.

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Received: 2 February 2024 / Accepted: 27 April 2024 Published online: 08 May 2024

References

- Yan S, Luo Z, Li Z, Wang Y, Tao J, Gong C, Liu X. Improving Cancer Immunotherapy outcomes using biomaterials. Angew Chem Int Ed Engl. 2020;59:17332–43.
- Merad M, Sathe P, Helft J, Miller J, Mortha A. The dendritic cell lineage: Ontogeny and function of dendritic cells and their subsets in the steady state and the Inflamed setting. Annu Rev Immunol. 2013;31:563–604.
- Liu J, Liew SS, Wang J, Pu K. Bioinspired and Biomimetic Delivery platforms for Cancer vaccines. Adv Mater 2021:e2103790.
- Li WH, Li YM. Chemical strategies to Boost Cancer vaccines. Chem Rev. 2020;120:11420–78.
- Jiang H, Wang Q, Sun X. Lymph node targeting strategies to improve vaccination efficacy. J Control Release. 2017;267:47–56.
- Wang Q, Wang Z, Sun X, Jiang Q, Sun B, He Z, Zhang S, Luo C, Sun J. Lymph node-targeting nanovaccines for cancer immunotherapy. J Control Release. 2022;351:102–22.
- Chen F, Wang Y, Gao J, Saeed M, Li T, Wang W, Yu H. Nanobiomaterial-based vaccination immunotherapy of cancer. Biomaterials. 2021;270:120709.
- Su T, Liu X, Lin S, Cheng F, Zhu G. Ionizable polymeric nanocarriers for the codelivery of bi-adjuvant and neoantigens in combination tumor immunotherapy. Bioact Mater. 2023;26:169–80.
- Du Y, Song T, Wu J, Gao XD, Ma G, Liu Y, Xia Y. Engineering mannosylated pickering emulsions for the targeted delivery of multicomponent vaccines. Biomaterials. 2022;280:121313.
- Ehrchen JM, Roth J, Roebrock K, Varga G, Domschke W, Newberry R, Sorg C, Müller-Tidow C, Sunderkötter C, Kucharzik T, Spahn TW. The absence of cutaneous lymph nodes results in a Th2 response and increased susceptibility to Leishmania major infection in mice. Infect Immun. 2008;76:4241–50.
- Wculek SK, Cueto FJ, Mujal AM, Melero I, Krummel MF, Sancho D. Dendritic cells in cancer immunology and immunotherapy. Nat Rev Immunol. 2020;20:7–24.
- Jia X, Chen H, Wu M, Wang L, Li T, Ma J, Yi X, Tan P, Zheng P, Du J. A biodegradable Antigen Nanocapsule promotes Anti-tumor Immunity via the cGAS-STING pathway. Adv Funct Mater 2023.
- Wang Y, Zhao Q, Zhao B, Zheng Y, Zhuang Q, Liao N, Wang P, Cai Z, Zhang D, Zeng Y, Liu X. Remodeling Tumor-Associated neutrophils to enhance dendritic cell-based HCC Neoantigen Nano-Vaccine Efficiency. Adv Sci (Weinh). 2022;9:e2105631.

- Jin L, Yang D, Song Y, Li D, Xu W, Zhu Y, Xu CF, Lu Y, Yang X. In situ programming of Nanovaccines for Lymph Node-targeted delivery and Cancer immunotherapy. ACS Nano 2022.
- Chu Y, Qian L, Ke Y, Feng X, Chen X, Liu F, Yu L, Zhang L, Tao Y, Xu R, et al. Lymph node-targeted neoantigen nanovaccines potentiate antitumor immune responses of post-surgical melanoma. J Nanobiotechnol. 2022;20:190.
- Zhang H, Zhang Y, Hu H, Yang W, Xia X, Lei L, Lin R, Li J, Li Y, Gao H. In situ tumor vaccine for Lymph Nodes Delivery and Cancer Therapy based on small size Nanoadjuvant. Small 2023:e2301041.
- 17. Liu H, Hu Z, Chen H, Yan Y, Le Z, Wei C, Cao W, Chen T, Chen Y, Liu L. Selfdegradable poly(β -amino ester)s promote endosomal escape of antigen and agonist. J Controlled Release. 2022;345:91–100.
- 18. Zhu G, Zhang F, Ni Q, Niu G, Chen X. Efficient nanovaccine delivery in Cancer Immunotherapy. ACS Nano. 2017;11:2387–92.
- Nakamura T, Harashima H. Dawn of lipid nanoparticles in lymph node targeting: potential in cancer immunotherapy. Adv Drug Deliv Rev. 2020;167:78–88.
- Scheetz L, Park KS, Li Q, Lowenstein PR, Castro MG, Schwendeman A, Moon JJ. Engineering patient-specific cancer immunotherapies. Nat Biomed Eng. 2019;3:768–82.
- Harari A, Graciotti M, Bassani-Sternberg M, Kandalaft LE. Antitumour dendritic cell vaccination in a priming and boosting approach. Nat Rev Drug Discovery. 2020;19:635–52.
- Kim H, Uto T, Akagi T, Baba M, Akashi M. Amphiphilic poly(amino acid) nanoparticles induce size-dependent dendritic cell maturation. Adv Funct Mater. 2010;20:3925–31.
- Foged C, Brodin B, Frokjaer S, Sundblad A. Particle size and surface charge affect particle uptake by human dendritic cells in an in vitro model. Int J Pharm. 2005;298:315–22.
- He C, Hu Y, Yin L, Tang C, Yin C. Effects of particle size and surface charge on cellular uptake and biodistribution of polymeric nanoparticles. Biomaterials. 2010;31:3657–66.
- Wang J, Wang Y, Qiao S, Mamuti M, An H, Wang H. In situ phase transitional polymeric vaccines for improved immunotherapy. Natl Sci Rev. 2022;9:nwab159.
- Qin H, Zhao R, Qin Y, Zhu J, Chen L, Di C, Han X, Cheng K, Zhang Y, Zhao Y, et al. Development of a Cancer Vaccine using in vivo click-Chemistry-mediated active Lymph Node Accumulation for Improved Immunotherapy. Adv Mater. 2021;33:e2006007.
- Wang W, Chen X, Li J, Jin Q, Jin HJ, Li X. Hollow MnO2 nanoparticles loaded with functional genes as Nanovaccines for Synergistic Cancer Therapy. ACS Appl Nano Mater. 2022;5:10537–47.

- Huang L, Peng S, Liu Z, Zhang J, Liu N, Lin J. Natural blood plasma-based hydrogels as tumor vaccines delivery systems to enhance biomimetic recruitment of antigen presenting cells for tumor immunotherapy. Mater Today Bio. 2022;17:100497.
- 29. Zhu W, Dong Z, Fu T, Liu J, Chen Q, Li Y, Zhu R, Xu L, Liu Z. Modulation of Hypoxia in Solid Tumor Microenvironment with MnO2 nanoparticles to enhance photodynamic therapy. Adv Funct Mater. 2016;26:5490–8.
- Gao F, Tang Y, Liu WL, Zou MZ, Huang C, Liu CJ, Zhang XZ. Intra/Extracellular lactic acid exhaustion for synergistic metabolic therapy and immunotherapy of tumors. Adv Mater. 2019;31:e1904639.
- Su Q, Liu Z, Du R, Chen X, Chen L, Fu Z, Luo X, Yang Y, Shi X. Facile preparation of a metal-phenolic network-based lymph node targeting nanovaccine for antitumor immunotherapy. Acta Biomater 2023.
- Liu X, Liao G, Zou L, Zheng Y, Yang X, Wang Q, Geng X, Li S, Liu Y, Wang K. Construction of Bio/Nanointerfaces: stable gold nanoparticle bioconjugates in Complex systems. ACS Appl Mater Interfaces. 2019;11:40817–25.
- Mei LP, Jiang XY, Yu XD, Zhao WW, Xu JJ, Chen HY. Cu Nanoclusters-Encapsulated liposomes: toward sensitive liposomal photoelectrochemical immunoassay. Anal Chem. 2018;90:2749–55.
- Byvaltsev VA, Bardonova LA, Onaka NR, Polkin RA, Ochkal SV, Shepelev VV, Aliyev MA, Potapov AA. Acridine Orange: a review of Novel Applications for Surgical Cancer Imaging and Therapy. Front Oncol 2019, 9.
- Wang C, Guan Y, Lv M, Zhang R, Guo Z, Wei X, Du X, Yang J, Li T, Wan Y, et al. Manganese increases the sensitivity of the cGAS-STING pathway for doublestranded DNA and is required for the Host Defense against DNA viruses. Immunity. 2018;48:675–e687677.
- Mackenzie KJ, Carroll P, Martin C-A, Murina O, Fluteau A, Simpson DJ, Olova N, Sutcliffe H, Rainger JK, Leitch A, et al. cGAS surveillance of micronuclei links genome instability to innate immunity. Nature. 2017;548:461–5.
- Richards DM, Sefrin JP, Gieffers C, Hill O, Merz C. Concepts for agonistic targeting of CD40 in immuno-oncology. Hum Vaccin Immunother. 2020;16:377–87.
- Zhang J, Fan B, Cao G, Huang W, Jia F, Nie G, Wang H. Direct presentation of Tumor-Associated antigens to induce adaptive immunity by personalized dendritic cell-mimicking nanovaccines. Adv Mater 2022;e2205950.

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